

Effects of Sleep-disordered Breathing on Cerebrovascular Regulation

A Population-based Study

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Rationale: Cerebrovascular regulation is impaired in patients with moderate to severe obstructive sleep apnea; however, it is unknown whether this impairment exists in individuals with less severe sleep-disordered breathing.

Objectives: To test the hypothesis that cerebrovascular responses to hypercapnia are attenuated in a nonclinical population-based cohort.

Methods: A rebreathing test that raised end-tidal CO₂ tension by 10 mm Hg was performed during wakefulness in 373 participants of the Wisconsin Sleep Cohort.

Measurements and Main Results: We measured cerebral flow velocity (transcranial Doppler ultrasound); heart rate (electrocardiogram); blood pressure (photoplethysmograph); ventilation (pneumotachograph); and end-tidal CO₂ (expired gas analysis). Cerebrovascular CO₂ responsiveness was quantified as the slope of the linear relationship between flow velocity and end-tidal CO₂ during rebreathing. Linear regression analysis was performed using cerebrovascular CO₂ responsiveness as the outcome variable. Main independent variables were the apnea-hypopnea index and the mean level of arterial oxygen saturation during sleep. We observed a positive correlation between cerebrovascular CO₂ responsiveness and the mean level of oxygen saturation during sleep that was statistically significant in unadjusted analysis and after adjustment for known confounders and the increase in arterial pressure during rebreathing. Each 5% decrease in Sa_o₂ during sleep predicted a decrease in cerebrovascular reactivity of 0.4 ± 0.2 cm/second/mm Hg P_{ET}CO₂. In contrast, the negative correlation between cerebrovascular CO₂ responsiveness and apnea-hypopnea index was statistically significant only in the unadjusted analysis.

Conclusions: Hypercapnic vasodilation in the cerebral circulation is blunted in individuals with sleep-disordered breathing. This impairment is correlated with hypoxemia during sleep.

Keywords: sleep apnea syndromes; cerebrovascular circulation; blood flow velocity; hypercapnia; endothelial function

Individuals with obstructive sleep apnea (OSA) syndrome are at increased risk for cardiovascular disease, including hypertension and stroke (1–3); however, the underlying mechanisms remain obscure. Putative links between OSA and stroke include

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AT A GLANCE COMMENTARY

Scientific Knowledge on the Subject

Moderate to severe obstructive sleep apnea is characterized by impaired endothelium-dependent vasodilation in the cerebral circulation.

What This Study Adds to the Field

This study demonstrates the presence of a similar impairment across a wider spectrum of sleep-disordered breathing in the general adult population.

oxidative stress (4), coagulopathies (5–7), thromboembolism associated with atrial fibrillation (8) and patent foramen ovale (9), and carotid atherosclerosis caused by snoring-related vibration (10). Structural abnormalities involving extracranial cerebral arteries (e.g., increased carotid intima-media thickness and augmented carotid-femoral pulse wave velocity) have been documented in patients with moderate to severe OSA (11–13). In addition, functional responses of intracranial cerebral arteries to CO₂, a powerful vasodilator in the cerebral circulation, are greatly attenuated (14–16).

The clinical significance of blunted hypercapnic vasodilation is unknown; however, previous investigators have observed an association between cerebral CO₂ reactivity and endothelial function in the forearm (17), a biomarker known to be a strong predictor of cardiovascular disease risk (18–20). In addition, impaired vascular responsiveness to CO₂ may exacerbate breathing instability during sleep. Because hypercapnic vasodilation minimizes changes in brain PCO₂ during fluctuations in arterial PCO₂, reductions in vascular reactivity could exaggerate the accumulation and also the washout of CO₂ from central chemoreceptors during fluctuations in ventilation. Thus, impaired vascular response to hypercapnia is a potential contributor to both the causes and the consequences of sleep-disordered breathing (SDB).

Current knowledge of the effects of SDB on cerebrovascular function is derived from clinic-based samples of individuals with relatively severe SDB. Similar impairments have not been documented across the spectrum of SDB severity, even though diminished endothelial function in the forearm has been demonstrated in epidemiologic studies (21, 22). Therefore, we sought to test the hypothesis that hypercapnic vasodilation in the cerebral circulation, an endothelium-dependent process, is blunted in individuals with SDB. Accordingly, we examined the relationship between SDB and cerebrovascular responsiveness to hypercapnia in a population-based cohort free of clinical selection biases. Some of the results of this study have been previously reported in abstract form (23).

METHODS

Subjects

Detailed sampling methods and characteristics of the Wisconsin Sleep Cohort Study have been described previously (24). Briefly, over the past 20 years, a random sample of 1,550 males and females was recruited from a sampling frame of payroll records of several Wisconsin state agencies to undergo polysomnographic examinations at 4-year intervals. Four hundred and twenty male and female participants of the Wisconsin Sleep Cohort Study who were scheduled to undergo follow-up evaluations during the years 2004–2008 were recruited to also participate in the present ancillary investigation of cerebrovascular function. Potential subjects were screened for current, serious medical problems via a self-reported history questionnaire that was followed-up by a physical examination, if necessary. In this manner, physician clearance was obtained for all subjects before participation. Twenty-one potential participants were deemed not healthy enough to undergo the rebreathing test, two declined participation after receiving an explanation of procedures, in seven instances there were equipment failures, and in 17 subjects we were unable to obtain an adequate Doppler signal. Characteristics of the remaining 373 subjects are shown in Table 1. The parent study and this subprotocol were approved by the University of Wisconsin-Madison's Health Sciences Institutional Review Board.

Measurements

Study participants completed overnight studies that included nocturnal polysomnography and other clinical tests. Information on medical history, current medication use, smoking, alcohol use, age, and other sociodemographic factors was obtained by interview and questionnaire. Body habitus measurements were made using standard procedures (25). Body mass index (BMI) was calculated from measured weight and height (kilogram per square meter). Insulin sensitivity was estimated using homeostatic model assessment (26). Daytime sleepiness was measured by the Epworth Scale (27). Blood pressure was measured with arm cuff sphygmomanometry in the seated position according to established guidelines (28). The average of two consecutive blood pressure measurements was computed for each subject.

Sleep-disordered breathing. An 18-channel polysomnography recording system (Polygraph model 78, Grass Instruments, Quincy, MA) was used to record sleep stage, and respiratory and cardiovascular variables. Electroencephalography, electrooculography, and chin electromyography were used to score sleep stage for each 30-second epoch using standard criteria (29). Arterial oxyhemoglobin saturation (SaO_2) was measured by pulse oximetry (Ohmeda 3740, Englewood, CO). Oral and nasal airflow were measured using thermocouples (ProTec, Hendersonville, TN). Nasal air pressure was measured with a pressure

transducer (Validyne, Northridge, CA). Thoracic cage and abdominal respiratory motion was measured with inductance plethysmography (Respirace, Ambulatory Monitoring, Ardsley, NY). These signals were used to identify SDB events. Apnea was defined as cessation of airflow lasting greater than or equal to 10 seconds. Hypopnea was defined as a decrease in tidal volume (plethysmograph signal) accompanied by a greater than or equal to 4% reduction in SaO_2 . The apnea-hypopnea index (AHI) was defined as the average number of apneas plus hypopneas per hour of objectively measured sleep. To compute mean SaO_2 during sleep, the pulse oximeter signal was sampled at 100 Hz and an average SaO_2 derived for each 30-second epoch. The average SaO_2 during all epochs of non-REM and REM sleep was recorded as the mean SaO_2 during sleep.

Medications. Two hundred and four participants were chronically treated with medications that could affect cerebrovascular CO_2 sensitivity, either by interfering with mechanisms of hypercapnic vasodilation or by affecting baseline cerebrovascular reactivity. The categories and number of participants who took these medications were as follows: antihypertensives ($n = 123$); statins ($n = 76$); estrogen ($n = 9$); allopurinol ($n = 10$); and nonsteroidal antiinflammatory agents ($n = 131$).

Cerebrovascular reactivity protocol. All subjects were studied during wakefulness in a semirecumbent position in the same room (ambient temperature, $24 \pm 1^\circ\text{C}$) at the same time of day (between 13:00 and 14:30 hours). A 2-MHz pulsed Doppler ultrasound system (Neurovision 500 M, Multigon Industries, Youkers, NY) was used to measure blood flow velocity in the proximal (M1) segment of the middle cerebral artery. We used previously published search techniques (30) to insonate the artery through the right temporal window in most subjects. In a small fraction of subjects, we used the left temporal window when an adequate signal could not be obtained on the right side. After the quality of the signal was maximized, the Doppler probe was secured using a headband device to provide a fixed angle of insonation. Heart rate was measured from the electrocardiogram. Beat-by-beat arterial pressure was measured by photoelectric plethysmography (Finapres, Ohmeda, Louisville, CO). Ventilation was measured via a mouthpiece and pneumotachograph (Model 5719, Hans Rudolph, Kansas City, MO). End-tidal O_2 tension and end-tidal CO_2 tension ($\text{P}_{\text{ET}}\text{CO}_2$) were sampled from the mouthpiece and measured with infrared gas analyzers (Models CD3A and S-3A/I, Ametek, Pittsburgh, PA). Each of the physiologic signals was routed to a signal conditioner/amplifier module and a physiologic chart recorder (TA-4000, Gould, Cleveland, OH), and was digitized and stored on a personal computer (sampling rate, 120 Hz) for off-line analysis using custom-written software.

We used a modified Read rebreathing test (31) to assess cerebrovascular responses to hypercapnia. A 6-L anesthesia bag was attached by means of a two-way valve to a mouthpiece. Before initiation of the rebreathing test, this bag was filled with a volume of air equal to the

TABLE 1. DESCRIPTION OF SAMPLE (N = 373) BY SLEEP-DISORDERED BREATHING CATEGORY

	Apnea-Hypopnea Index Category						CPAP Users (n = 29)
	Total (n = 373)	<1 (n = 112)	1–4.9 (n = 100)	5–14.9 (n = 94)	15–29.9 (n = 25)	≥30 (n = 13)	
Continuous variables, mean (SD)							
Age, yr	60 (8)	58 (8)	61 (7)	61 (8)	63 (8)	58 (7)	59 (8)
Body mass index, kg/m ²	31 (6.9)	28 (4.7)	30 (6.4)	33 (6)	34 (7)	36 (8.7)	40 (6.9)
Waist:hip ratio	0.9 (0.1)	0.9 (0.1)	0.9 (0.1)	1 (0.1)	0.9 (0.1)	1 (0.1)	1 (0.1)
Alcoholic drinks, number per week	3.7 (4.7)	3.9 (4.6)	3.7 (4.3)	3.8 (5.3)	4.2 (5.6)	2.6 (4.2)	2.6 (4.4)
Sleep SaO_2 , %	94.9 (2)	95.8 (1.3)	95.2 (1.5)	94.7 (1.6)	93.8 (1.5)	92.2 (3.3)	93.5 (3.2)
Insulin sensitivity, HOMA model	3.6 (4.5)	2.3 (1.6)	3.1 (2.6)	4.1 (4.1)	4.7 (5.6)	7.6 (11.6)	6.6 (7.8)
Binary variables, n (%)							
Current smoking	35 (9)	12 (11)	13 (13)	4 (4)	1 (4)	3 (23)	2 (7)
Sex, male	216 (58)	56 (50)	51 (51)	67 (71)	14 (56)	9 (69)	20 (70)
Sleepiness, Epworth >10*	103 (31)	27 (25)	31 (32)	35 (38)	4 (16)	6 (50)	15 (52)
Cardiovascular disease†	40 (11)	10 (29)	9 (9)	10 (11)	4 (16)	3 (23)	4 (14)
Hypertension	187 (50)	46 (41)	42 (42)	55 (59)	16 (64)	7 (54)	22 (76)
Diabetes†	38 (10)	6 (5)	7 (7)	14 (15)	3 (12)	0 (0)	8 (28)

Definition of abbreviations: CPAP = continuous positive airway pressure; HOMA = homeostatic model assessment.

* Epworth data not available in 10 participants.

† Obtained by participant self-report.

subject's predicted vital capacity plus 1 L that had a gas composition of 3% CO₂ and 40% O₂. Predicted vital capacity was calculated using the following equations (32):

$$\begin{aligned} \text{Males: } & 0.052 \cdot \text{height (cm)} - 0.022 \cdot \text{age} - 3.6 \\ \text{Females: } & 0.047 \cdot \text{height (cm)} - 0.029 \cdot \text{age} - 2.9. \end{aligned}$$

The test began with a baseline period of room air breathing through the mouthpiece with the nose occluded in which at least 4 minutes of stable normoxic, normocapnic breathing were recorded. After the baseline recordings were complete, the valve was turned to allow rebreathing from the bag. The P_{ET}CO₂ level of the first breath from the bag was noted, and rebreathing continued until P_{ET}CO₂ reached +10 mm Hg above this level. In most subjects, this level was reached within 2.5 minutes. Then, the valve was opened to room air, and after the first room air breath, the mouthpiece and noseclip were removed. Typical responses to this rebreathing test are shown in Figure 1.

Calculation of Outcome Variables

All signals were analyzed using custom-written software. Cerebral flow velocity for each cardiac cycle was determined by integrating the Doppler signal and dividing by the length of the cycle (i.e., velocity-time integral). Mean arterial pressure (MAP) was calculated as one third pulse pressure plus diastolic pressure. Within-breath averages were computed for velocity-time integral, heart rate, and MAP. To quantify vascular responsiveness to CO₂, we performed breath-by-breath linear regression analysis of velocity-time integral versus P_{ET}CO₂. The slope of this relationship was used to make between-subject comparisons of cerebrovascular CO₂ responsiveness (CCR) (centimeters per seconds per millimeters of mercury P_{ET}CO₂). The day-to-day reliability of these measurements, assessed in nine healthy subjects, was good (intraclass correlation coefficient = 0.80). Linear regression analysis was also used to determine the change, per millimeter of mercury P_{ET}CO₂, in secondary outcome measures of MAP, heart rate, and ventilation during rebreathing. Quantification of physiologic variables associated with the rebreathing test was performed by one of two study personnel. To assess the reliability of our analysis procedures, we performed duplicate quantifications for every 15th subject tested. This examination revealed excellent repeatability (intraclass correlation coefficients >0.99).

Statistical Analysis

The distributions of all variables assessed in the Cerebrovascular Reactivity Protocol were approximately normal. We performed linear regression analyses with CCR as the primary outcome variable. The MAP, heart rate, and ventilatory responses during rebreathing were secondary outcome variables. We examined SDB severity as the independent variable, using two different representations. One was the AHI, categorized into severity levels (level 1, AHI <1; level 2, AHI 1–4.9; level 3, AHI 5–14.9; level 4, 15–29.9; and level 5, AHI ≥30). We tested this categorical variable using a linear trend test. We also examined log-transformed AHI (log[AHI+1]) as a continuous variable. The other measure of SDB severity was mean level of SaO₂ during sleep, a continuous variable. In this SaO₂ analysis, we excluded individuals with lung disease (those reporting a diagnosis of emphysema or use of β agonist, adrenal glucocorticoid, methylxanthine, leukotriene inhibitor, or mast cell stabilizer medications). In all linear re-

gression analyses, we excluded subjects who were current users of nasal continuous positive airway pressure (CPAP) (n = 29) because their polysomnographic data are not accurate reflections of the amount of SDB experienced on a nightly basis.

Initially, we examined unadjusted relationships. Secondly, we adjusted for age; sex; BMI; waist-to-hip ratio; current smoking; alcohol use (drinks per week); and the presence of diabetes. We adjusted for these potential confounders because of their known influence on SDB and endothelial function (33–38). In addition, for CCR, we also examined models that included an adjustment for the increase in MAP during rebreathing. It was necessary to adjust for MAP because it is an indicator of cerebral perfusion pressure, an important determinant of cerebral blood flow (39). Finally, we also examined two-way interactions between SDB:CCR relationships and age, sex, and excessive daytime sleepiness.

We used β coefficients from the model and population means for the confounding variables to estimate least square means of our outcomes for the AHI severity level categories. We used the β coefficient to estimate the effect of log AHI and mean level of oxygen saturation. Chi-square *t* tests were used to assess statistical significance and *P* values less than 0.05 were considered statistically significant for main effects. For interaction terms, we used a more conservative α level of *P* less than 0.01. SAS software (version 9.1.3, SAS Institute, Cary, NC) was used for all analysis.

RESULTS

Seventeen of 390 participants (5 males and 12 females) were excluded from analysis because of inability to obtain an adequate Doppler signal. These participants tended to have higher BMI, but did not differ from the remaining subjects in terms of AHI, presence of diabetes, or history of cardiovascular disease (data not shown).

Baseline Cardiovascular and Respiratory Variables

Summary data for cardiovascular and respiratory variables measured before the rebreathing test are shown in Table 2. Minute ventilation was somewhat elevated in patients in the highest AHI category and in CPAP users relative to other categories; however, P_{ET}CO₂ was comparable in all groups.

Cardiovascular and Respiratory Variables During Rebreathing

The rebreathing protocol was generally well-tolerated. We did not observe signs of hemodynamic instability in any participant. Transient breathlessness was the most commonly reported symptom. The rebreathing test elicited, on average, increases in heart rate of one beat per minute, MAP of 12 mm Hg, and minute ventilation of 17 liters per minute. Summary data for these variables and CCR are shown in Table 3.

We observed a significant positive correlation between CCR and mean SaO₂ during sleep (Table 4 and Figure 2). This relationship was evident in the unadjusted analysis (*P* = 0.013) and it persisted after adjustments for age; sex; BMI; alcohol consumption; smoking; diabetes; waist-to-hip ratio; and

TABLE 2. BASELINE VALUES FOR PHYSIOLOGIC VARIABLES BY SLEEP-DISORDERED BREATHING CATEGORY*

	Apnea-Hypopnea Index Category						CPAP Users (n = 29)
	Total (n = 373)	<1 (n = 112)	1–4.9 (n = 100)	5–14.9 (n = 94)	15–29.9 (n = 25)	≥30 (n = 13)	
P _{ET} CO ₂ , mm Hg	40 (4)	40 (4)	40 (3)	40 (3)	40 (3)	40 (7)	39 (3)
Ventilation, L/min	8.3 (2.1)	7.7 (1.9)	7.8 (1.6)	8.7 (2)	8.4 (2)	10.6 (3.2)	9.8 (2.5)
Heart rate, beats/min	68 (11)	68 (11)	68 (11)	67 (10)	72 (9)	74 (12)	69 (13)
Systolic pressure, mm Hg	122 (14)	119 (14)	122 (13)	125 (14)	127 (10)	125 (11)	127 (15)
Diastolic pressure, mm Hg	78 (9)	76 (9)	78 (7)	78 (10)	80 (11)	80 (8)	78 (8)

Definition of abbreviations: CPAP = continuous positive airway pressure; P_{ET}CO₂, end-tidal CO₂ tension.

* Values shown are means (SD).

TABLE 3. CARDIOVASCULAR AND RESPIRATORY VARIABLES MEASURED DURING REBREATHING BY SLEEP-DISORDERED BREATHING CATEGORY*

	Apnea-Hypopnea Index Category						CPAP users (n = 29)
	Total (n = 373)	<1 (n = 112)	1-4.9 (n = 100)	5-14.9 (n = 94)	15-29.9 (n = 25)	≥30 (n = 13)	
CCR, cm/s/mm Hg	2.3 (1)	2.4 (0.9)	2.4 (1.1)	2.1 (0.9)	2.3 (0.8)	2 (0.8)	2.3 (1)
Change in MAP, mm Hg/mm Hg	1.2 (1)	1.3 (1)	1.2 (1)	1.1 (1)	1.2 (0.7)	0.8 (0.8)	1 (1)
Change in HR, beats/min/mm Hg	0.1 (0.6)	0.2 (0.6)	0.2 (0.5)	0.1 (0.6)	0.1 (0.4)	-0.2 (0.5)	-0.0 (0.5)
HCVr, L/min/mm Hg	1.7 (1.1)	1.7 (1)	1.6 (1)	1.8 (1)	1.3 (0.9)	1.2 (1)	2 (1.9)

Definition of abbreviations: CCR = cerebrovascular CO₂ responsiveness; CPAP = continuous positive airway pressure; HCVr = hypercapnic ventilatory response; HR = heart rate; MAP = mean arterial pressure.

* Values shown are means (SD).

MAP increase during rebreathing ($P = 0.014$). The β coefficient associated with the model indicates that for each 5% decrease in mean SaO₂ during sleep, CCR was reduced by 0.4 cm per second per mm Hg (40% of the population SD for CCR). No two-way interactions were observed between the SaO₂-CCR relationship and age, sex, or sleepiness. Adjustment of the statistical model for several categories of medications that are putative confounders of the SaO₂-CCR relationship (antihypertensive agents, statins, estrogen, allopurinol, or cyclooxygenase inhibitors) did not affect β coefficients or P values, nor did further adjustment for insulin sensitivity (data not shown). No relationships were observed between mean SaO₂ during sleep and increase in MAP during rebreathing ($P = 0.782$); change in heart rate during rebreathing ($P = 0.995$); or hypercapnic ventilatory response ($P = 0.497$).

We also evaluated the association between CCR and AHI (Table 5). When AHI category was used as a trend variable, the association was nearly significant in the unadjusted analysis ($P = 0.050$); however, when alcohol consumption, smoking, diabetes, and waist-to-hip ratio were added to the model, the correlation was not significant ($P = 0.111$). The association between CCR and AHI category was also nonsignificant when MAP increase during rebreathing was added to the model ($P = 0.179$). Qualitatively similar results were found when using continuous AHI (log[AHI+1]) instead of categorical AHI. The unadjusted coefficient (SE) for CCR regressed on log(AHI+1) was -0.10 (0.05) ($P = 0.033$); with adjustment for age, sex, BMI, waist-to-hip ratio, current smoking, diabetes diagnosis, and alcohol consumption, the coefficient (SE) for log(AHI+1) was -0.10 (0.05) ($P = 0.073$). When the change in MAP during rebreathing was added to the model, the coefficient (SE) for log(AHI+1) was -0.08 (0.05) ($P = 0.123$). Further adjustment for insulin sensitivity did not affect β

coefficients or P values; thus, we did not include insulin sensitivity in the final analysis. No two-way interactions were observed between the AHI-CCR relationship and age, sex, or sleepiness.

We observed an inverse relationship between AHI category and increase in MAP during rebreathing that was of borderline significance ($P = 0.079$). In contrast, there was no significant relationship between AHI and change in heart rate during rebreathing ($P = 0.208$) or hypercapnic ventilatory response ($P = 0.182$).

Although we did not include data from current CPAP users in our statistical models, we did assess cerebrovascular reactivity in these individuals. In current CPAP users, the mean value for CCR (2.3 ± 0.2) was lower than in individuals with AHI less than five but higher than in those with AHI greater than 30 (Table 3).

DISCUSSION

The major finding of this study is that hypercapnic vasodilation in the cerebral circulation, an exquisitely sensitive physiologic mechanism responsible for minimizing changes in brain tissue Pco₂ during fluctuations in arterial CO₂, is diminished, in graded fashion, across the continuum of mild to severe SDB. We observed a significant positive correlation between the mean level of SaO₂ during sleep and cerebrovascular CO₂ reactivity. In contrast, AHI, regardless of whether it was represented as a categorical or continuous variable, was not statistically significantly associated with cerebrovascular CO₂ reactivity. Although we cannot infer causation from our observational data, we interpret these findings as indirect evidence that nocturnal hypoxemia contributes importantly to impaired cerebrovascular function in individuals with SDB.

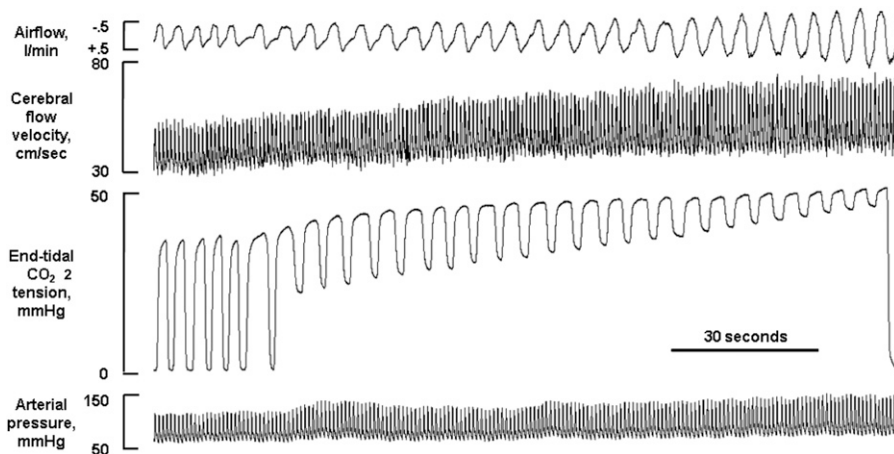


Figure 1. Physiologic record showing typical cardiovascular and respiratory responses to the rebreathing test.

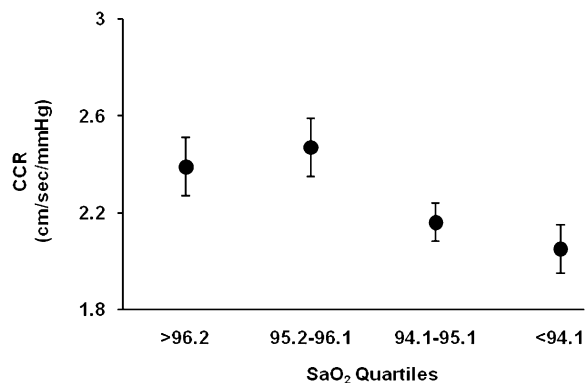


Figure 2. Cerebrovascular CO₂ reactivity (CCR) plotted as a function of SaO₂ during sleep. More severe sleep-disordered breathing, as indicated by lower mean sleep SaO₂, was associated with reduced CCR. Values shown are means \pm SE.

This conclusion is predicated on the assumption that reductions in SaO₂ during sleep were caused by SDB. Alternatively, SaO₂ may have been reduced secondary to lung disease. However, we believe this possibility was minimized because participants with a history of lung disease and those taking medications used to treat lung disease were excluded from this analysis. Also, our assumption that the reduction in CCR we observed in participants in the lower quartiles of nocturnal SaO₂ represents impaired hypercapnic vasodilation is valid only if the rebreathing test evoked comparable increases in MAP across all subject groups. This is a reasonable assumption because there was no correlation between nocturnal SaO₂ and MAP during rebreathing and because the SaO₂-CCR relationship was statistically significant both before and after adjustment for the increase in MAP. In contrast, the AHI-CCR relationship was confounded by between-group differences in MAP: a negative correlation of borderline significance was observed between AHI and MAP during rebreathing. Thus, it is not possible to discern whether CCR was lower in participants with higher AHI because of blunted hypercapnic vasodilation or whether CCR was lower secondary to smaller increases in cerebral perfusion pressure during rebreathing. The finding that the AHI-CCR relationship became statistically nonsignificant after adjustment for the increase in MAP during rebreathing points to the latter possibility. Our data are consistent in demonstrating that, across a wide spectrum of SDB, the mean level of SaO₂ during sleep better predicts the blunting of CO₂ reactivity than does the frequency of events (*i.e.*, AHI).

In contrast to the significant negative correlation between SDB and CCR in our subjects, ventilatory responses during rebreathing did not vary according to SaO₂ or AHI category. In one previous study, enhanced ventilatory responses to CO₂ were reported in OSA patients versus control subjects (40); however, several other studies have found no between-group differences (16, 41, 42). We speculate that much of the

variability in ventilatory responses to CO₂ is attributable to performance of these studies during wakefulness, when non-chemoreceptor, behavioral inputs have a substantial influence on respiratory output.

The present findings in a population-based sample free of clinical selection biases are consistent with our previous observations of diminished CCR in patients with moderate to severe OSA (16). The magnitude of CCR decrement in the present subjects who fell within the lowest versus the highest quartiles of nocturnal SaO₂ values was similar to that observed in our clinic-based sample (-17 versus -22%). Because the average CCR in CPAP users was enhanced relative to participants with untreated SDB and AHI greater than 30, the present findings suggest that SDB-related impairment in cerebrovascular function is reversible, at least in part, with treatment. This finding also agrees with our previous observations of patients with moderate to severe OSA (16). Nevertheless, because the average CCR in CPAP users was still somewhat diminished relative to that of participants with no SDB (AHI <5), the present data also suggest that CPAP does not provide full protection against this vascular consequence of SDB. A potential reason is that many individuals are not fully compliant with this treatment. Patients who are considered "CPAP compliant" use the device for as few as 4 hours on most nights (43-45). Thus, many of them remain exposed, for varying amounts of time, to the adverse effects of SDB and resultant intermittent hypoxemia.

The present findings also parallel two previous population-based studies that used flow-mediated dilation in the forearm to assess vascular function (21, 22). All three studies found associations between vascular dysfunction and SDB severity. Consistent with the present findings, one previous study found that nocturnal SaO₂ was a more important predictor of vascular function than was AHI (21). The other previous study observed that SDB was associated with impaired vascular function in females, but not males (22). In the present study, the interaction between sex and SDB-associated vascular dysfunction was not statistically significant. Interestingly, a significant positive correlation was observed between vascular reactivity and alcohol consumption in one previous report (22). A similar correlation was not present in our study.

Mechanisms of SDB-induced Impairment in Cerebrovascular Reactivity

Hypercapnic vasodilation in the brain is a complex, endothelium-dependent process: nitric oxide, prostacyclin, and cytochrome P-450 metabolites have all been implicated (46-48). Endothelium-dependent dilation in the forearm is blunted in individuals with SDB (21, 49-51). The causes of this impairment are not well understood; however, oxidative stress (*i.e.*, imbalance between production of reactive oxygen species and antioxidant defenses) and inflammation are putative contributors. Both processes have been observed in patients with OSA (4), are

TABLE 4. BETA COEFFICIENTS AND P VALUES FOR UNADJUSTED AND ADJUSTED PREDICTION MODELS BASED ON CORRELATIONS BETWEEN MEAN SLEEP SaO₂ AND THE PRIMARY OUTCOME MEASURE

Mean sleep SaO ₂	Outcome Measure: Cerebrovascular CO ₂ Reactivity (cm/s/mm Hg P _{ET} CO ₂)					
	Model 1		Model 2		Model 3	
	Unadjusted		Adjusted for age, sex, body mass index, waist:hip ratio, current smoking, drinks per week, diabetes		Adjusted (Model 2 adjustments + increase in MAP)	
	Beta (SE)	P Value	Beta (SE)	P Value	Beta (SE)	P Value
	0.08 (0.03)	0.013	0.08 (0.04)	0.019	0.09 (0.04)	0.014

TABLE 5. MEAN VALUES (SE) FOR CEREBROVASCULAR CO₂ REACTIVITY IN THE FIVE SLEEP-DISORDERED BREATHING CATEGORIES

AHI	Outcome Measure: Cerebrovascular CO ₂ Reactivity (cm/s/mm Hg P _{ET} CO ₂)		
	Model 1	Model 2	Model 3
	Unadjusted	Adjusted for Age, Sex, Body Mass Index, Waist:Hip Ratio, Current Smoking, Drinks Per Week, Diabetes	Adjusted (Model 2 adjustments + MAP Slope)
1: AHI <1	2.39 (0.09)	2.39 (0.10)	2.37 (0.10)
2: AHI 1 to <5	2.36 (0.10)	2.34 (0.10)	2.35 (0.10)
3: AHI 5 to 14.9	2.10 (0.10)	2.14 (0.11)	2.15 (0.10)
4: AHI 15 to 29.9	2.34 (0.19)	2.29 (0.19)	2.30 (0.19)
5: AHI ≥ 30	1.96 (0.27)	2.02 (0.27)	2.07 (0.27)
P value for trend	0.050	0.111	0.179

Definition of abbreviations: AHI = apnea-hypopnea index; MAP = mean arterial pressure.

accompanied by decreased expression of endothelial nitric oxide synthase and increased expression of both nitrotyrosine and inducible nitric oxide synthase in venous endothelial cells (51), and are ameliorated by CPAP treatment (51). In addition, allopurinol treatment has been shown to normalize impaired flow-mediated dilation in patients with OSA (52), which suggests an important role for xanthine oxidase-derived superoxide. Excess superoxide would be expected to reduce the availability of nitric oxide by combining with it to form peroxynitrite. Peroxynitrite, in turn, could further limit nitric oxide via oxidation of tetrahydrobiopterin, a critical cofactor for endothelial nitric oxide synthase (53, 54). Peroxynitrite could also limit prostacyclin production by suppression of prostacyclin synthase (55). We speculate that the pathologic processes that interfere with endothelium-dependent vasodilation in the forearm also contribute to the observed blunting of hypercapnic vasodilation in the cerebral circulation.

Methodologic Considerations

Our conclusions regarding cerebrovascular responses are predicated on the assumption that Doppler measurements of flow velocity are reflective of volume flow, an assumption that is satisfied only when the cross-sectional area of the artery remains constant. We did not measure diameter; however, previous investigators have shown that middle cerebral artery diameter varies by less than or equal to 4% during changes in arterial pressure, CO₂ tension (56), or gravitational stress (57). In addition, velocity and volume flow through the middle cerebral artery are highly correlated (58). Also, one of our measures of SDB severity, AHI, has limited reliability, especially over a single night of observation. Nevertheless, with 373 subjects, we believe our study is adequately powered considering the known night-to-night variability (59).

In the absence of SaO₂ measurements during wakefulness and concurrent measurements of pulmonary function, individuals with lung disease were identified based on self-reported medical history and use of medications used to treat lung disease. We recognize that this imprecise method is a limitation of our study.

Finally, in this cross-sectional study, we cannot uncover the temporal nature of the relationship between SDB and blunted CCR. On one hand, SDB could cause impairment in reactivity via intermittent hypoxemia and attendant insults to vascular structure and function. However, diminished cerebrovascular CO₂ reactivity could cause or exacerbate SDB. Answers to these questions await longitudinal observations in population-based studies.

Clinical Significance of the Present Findings

Several previous reports suggest that the observed impairments in CCR may be clinically relevant. In patients with essential hypertension and diabetes mellitus, impaired CCR was corre-

lated with endothelial dysfunction in the forearm (17), a strong predictor of cardiovascular disease risk (18, 20). Because hypercapnic vasodilation in the cerebral circulation is evoked by substances produced in endothelial cells (46–48), we believe that CCR is a proxy measure of endothelial function and therefore may also be a predictor of cardiovascular risk. Diminished cerebrovascular responsiveness to CO₂ has been observed in patients with ischemic stroke (60) and those with multiple subcortical infarctions (61). Therefore, this functional impairment may play a pathogenetic role in cerebrovascular disease. Further, in patients with congestive heart failure, CCR was correlated with ejection fraction, prompting the speculation that depressed cerebrovascular reactivity may be responsible for cognitive impairments in patients with severe ventricular dysfunction (62). We have shown that CCR is reduced in patients with heart failure and central sleep apnea relative to patients with similar cardiac dysfunction but without central sleep apnea (63). Because CO₂ reactivity in the cerebral circulation minimizes changes in brain Pco₂ during fluctuations in arterial Pco₂, the observed compromise in cerebrovascular regulation may disturb breathing stability during sleep. Reductions in CCR could exacerbate breathing instability during sleep by exaggerating the accumulation and also the washout of CO₂ from central chemoreceptors during fluctuations in ventilation and arterial Pco₂.

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